



Microfluidic Detection of *Escherichia coli* in Macro Water Distribution System

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- **Motivation**

- Concern has recently been raised about vulnerability of water supply system to terrorist attack
 - Pathogenic contamination in drinking and irrigation water threatens the environment and public health
- Accurate and real-time risk assessment of biological agent is a critical issue
 - Developing quantitative sensor to monitor water quality
 - Improving accuracy in predicting transport phenomena of the biological agents in water distribution system

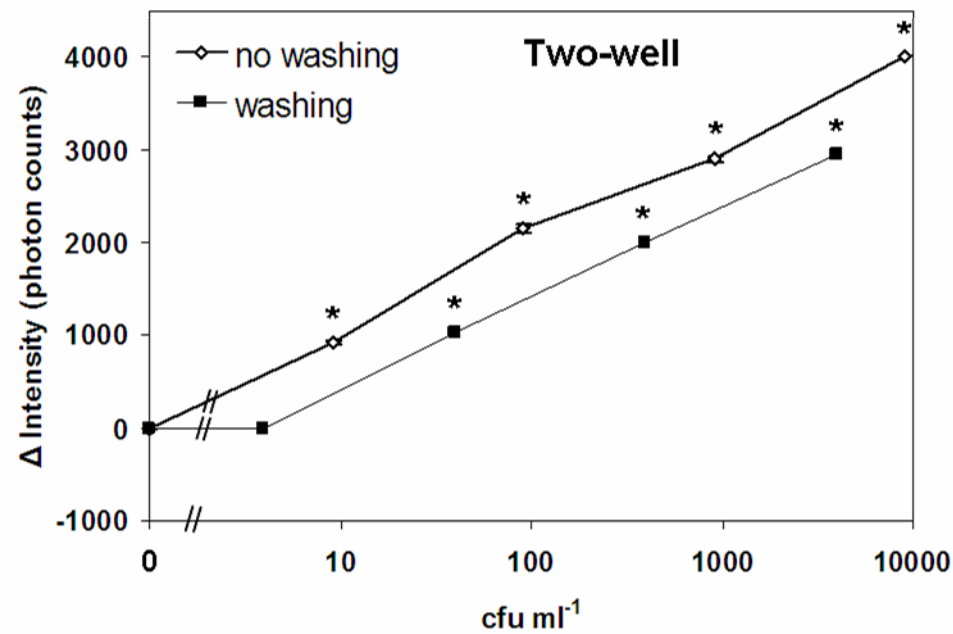
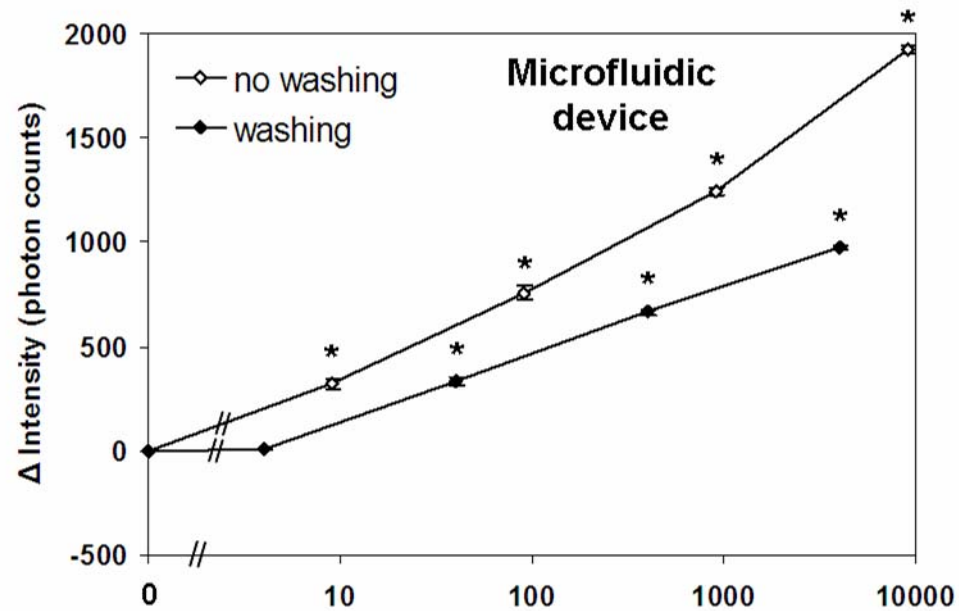


Previous studies

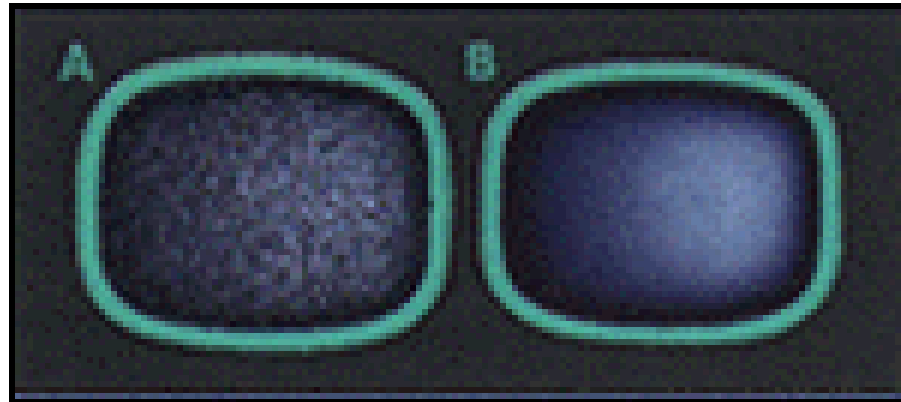


- Detecting waterborne pathogens in a microfluidic device

- More sensitive and faster detection than PCR or ELISA
- Lin et al., *Biomed. Microdev.* 6: 125 (2004)
 - Immunoassay for *E. coli* O157:H7 using colorimetric quantification in a PDMS microfluidic device (detection limit: 10 ng or 3×10^4 cells)
- Li and Su, *J. Rapid Meth. Autom. Microbiol.* 14: 96 (2006)
 - Capturing *E. coli* O157:H7 with the antibodies immobilized in a microfluidic device, followed by detection with a UV/vis spectrometer
- Han et al., *Biosens. Bioelectron.* doi:10.1016/j.bios.2007.11.013 (2008)
 - Real-time detection of viable *E. coli* only through light scattering of latex immunoagglutination in a microfluidic device (detection limit: 4 cfu per device)

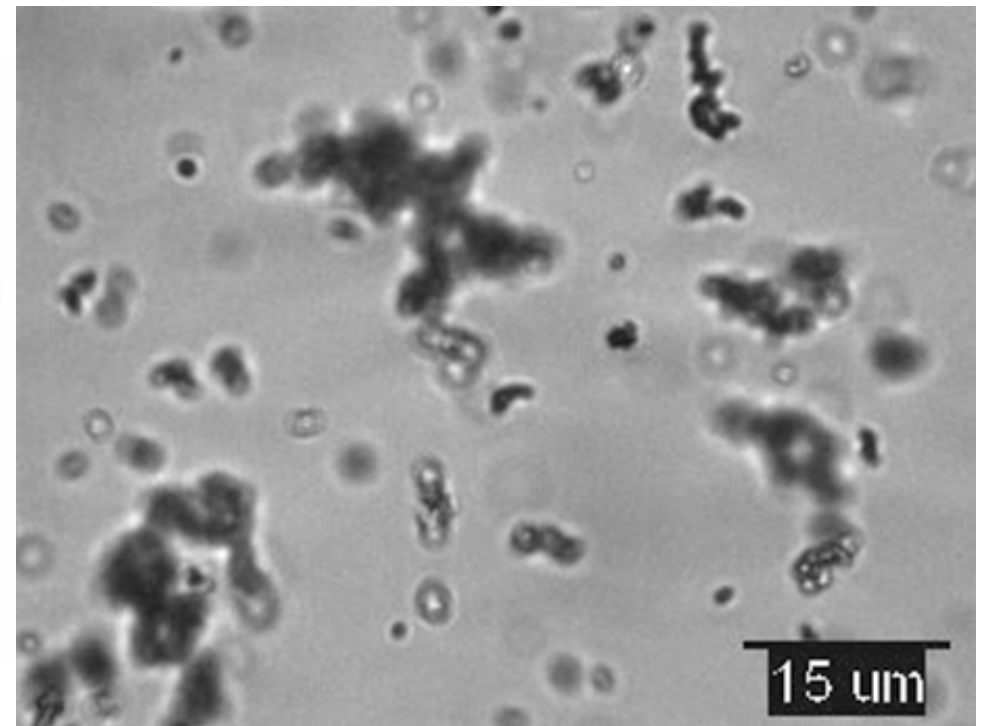
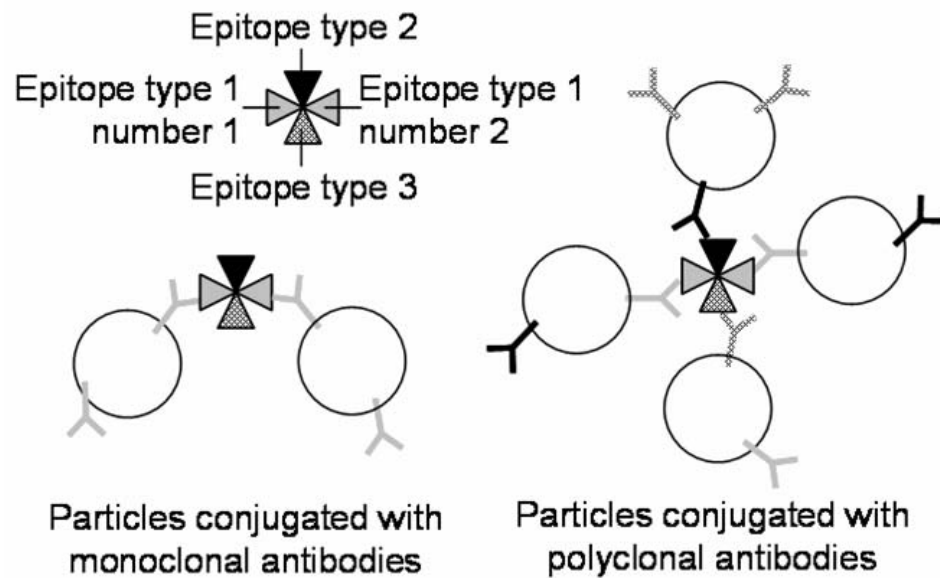


- What is latex agglutination test (LAT)?

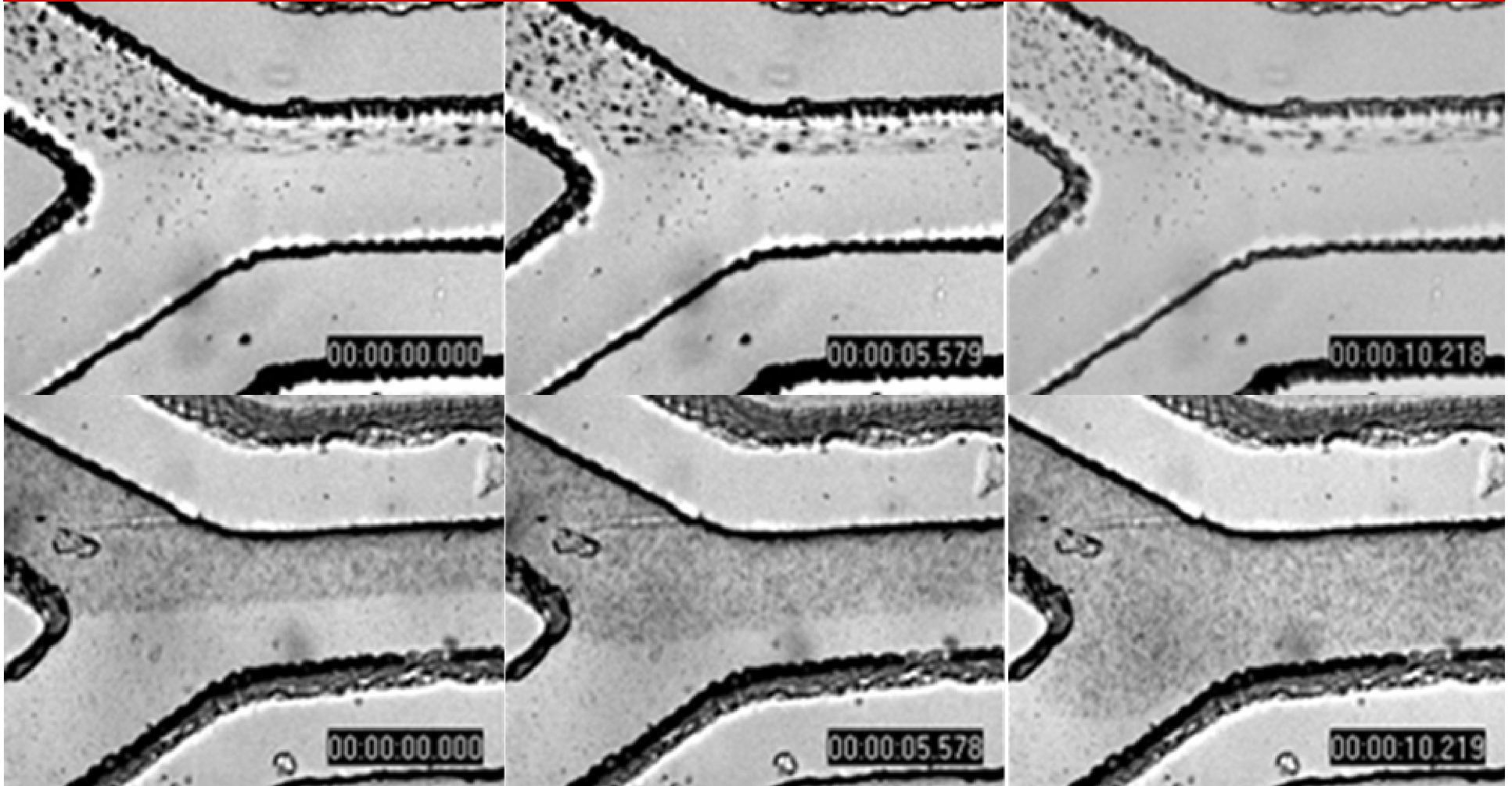


- Polymer microparticles, or latex, conjugated with antibodies, are mixed to target specimen.
- Existence of complementary antigens in the specimen results in connecting two or more particles, known as agglutination.
- This agglutination can visually identified.

- Particle immunoagglutination in microfluidics



- Particle immunoagglutination in microfluidics



Han et al. *Anal. Chim. Acta* 584: 252 (2007)



- Predicting transport phenomena of a pipe flow

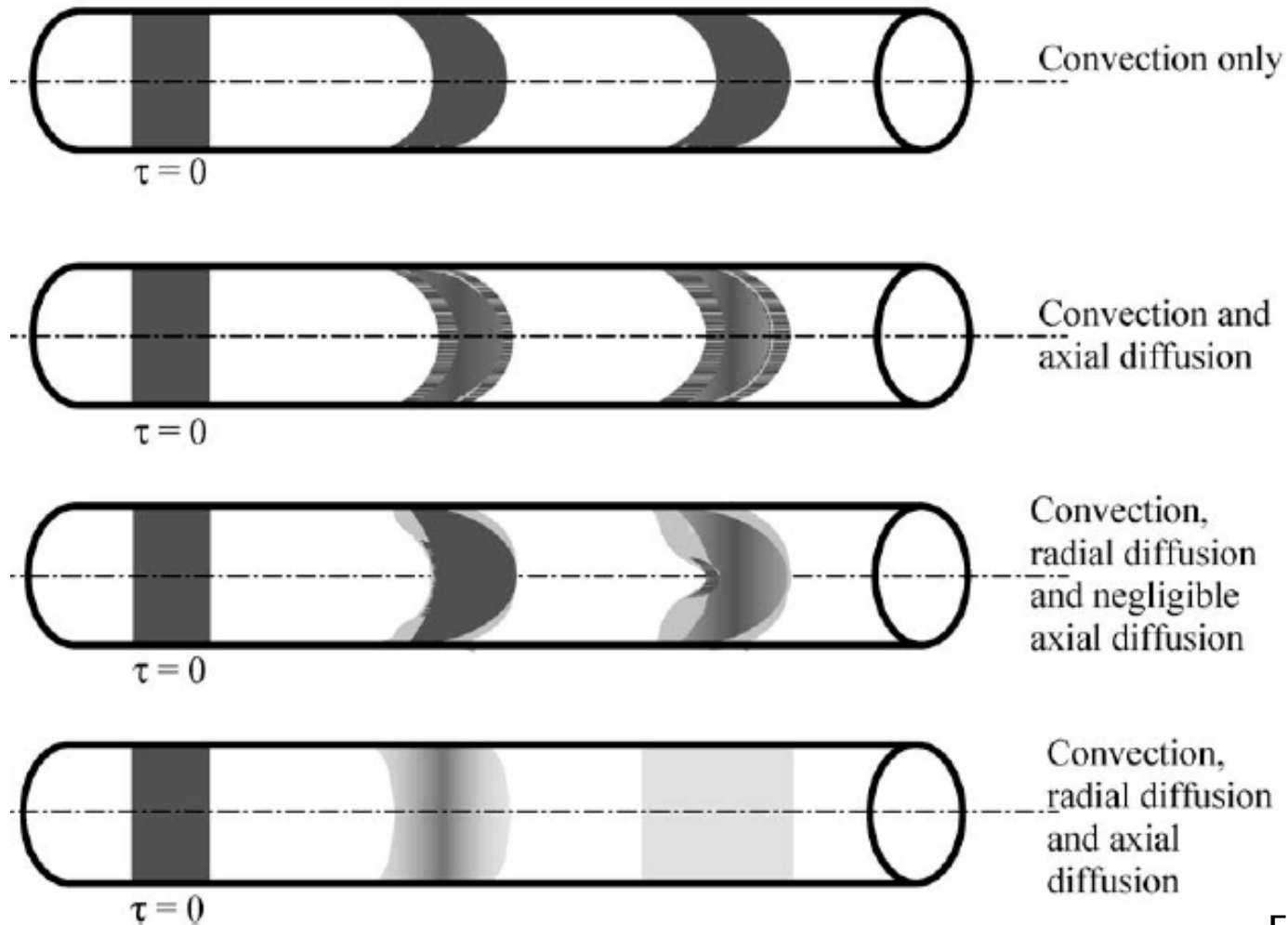
- Molecular transport in a pipe flow has been extensively studied since 1950s
- Taylor, *Proc. R. Soc. London A* 219: 186 (1953); 225: 473 (1954)
 - Analyzed the dispersion of salt injected into a capillary tube.
 - The axial dispersion model was valid when dimensionless time is much higher than 0.7 ($T = 4 D t/d^2$) and Peclet number is higher than 500 ($Pe = a u_0/D$)
 - D = molecular diffusion coefficient, t = elapsed time, d = inner diameter of a pipe, a = radius of a pipe, u_0 = maximum flow velocity
 - Concentration profile of salt tracer = symmetric in laminar flow regarding axial convection



- Predicting transport phenomena of a pipe flow

- Shanker and Lenhoff, *AIChE* 35: 2048 (1989)
 - Concentration profile of the tracer in a short pipe: asymmetric
 - Due to the combined effects of axial convection, radial diffusion, and axial diffusion
- Ekambara and Joshi, *Chem. Engin. Sci.* 59: 3929 (2004)
 - Developed a computational model for wider ranges of: T (10^{-8} ~ 10^2) and Pe (1 - 10^5)

- What are the axial convection, radial diffusion and axial diffusion?



Ekambara and Joshi (2004)



• Objectives

- Apply microfluidic system for detecting *E. coli* in laminar and turbulent pipe flows
 - Detection limit close to 10 CFU/ml
 - Monitor *E. coli* concentrations according to time variance (real-time detection; preferably <5 min per assay)
- Compare flow characteristics of *E. coli* and non-biological agent in a pipe
 - Light scattering signal from microfluidic system for *E. coli*
 - Viable *E. coli* counts (not real-time)
 - Salt concentration



Materials and method



• Materials

- Microparticles: 1 ml of 0.02% 0.92 μm highly carboxylated polystyrene particles
- Antibody: 1 ml of 1.023 $\mu\text{g ml}^{-1}$, anti-*E. coli* (polyclonal antibody developed in rabbit) for 33% surface coverage of antibody to microparticles
- 70 ml of 1.5 mg ml^{-1} salt (NaCl) as non-biological tracer

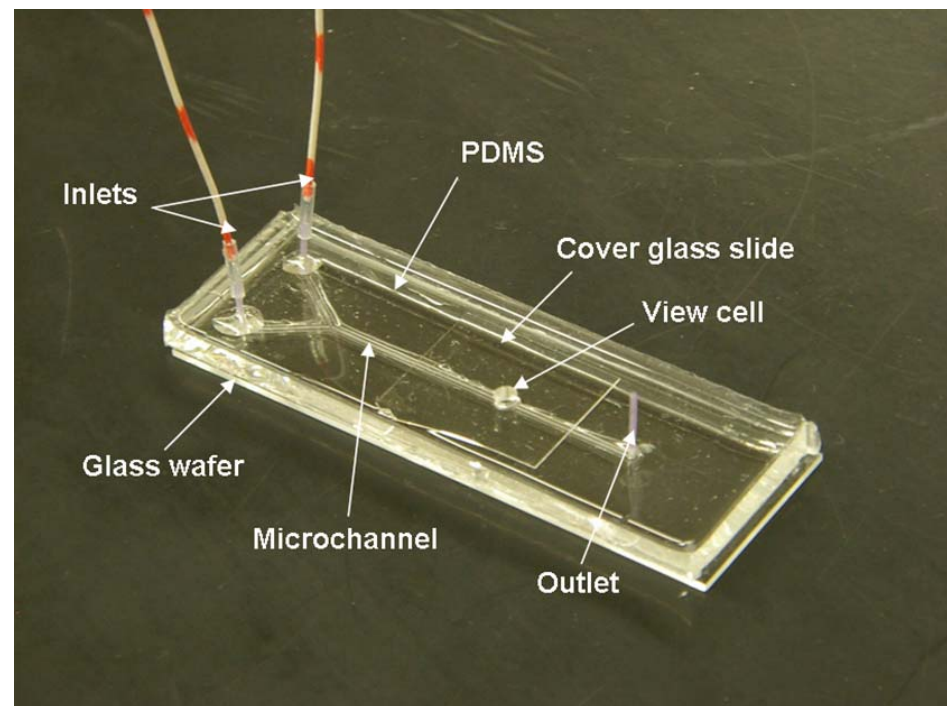
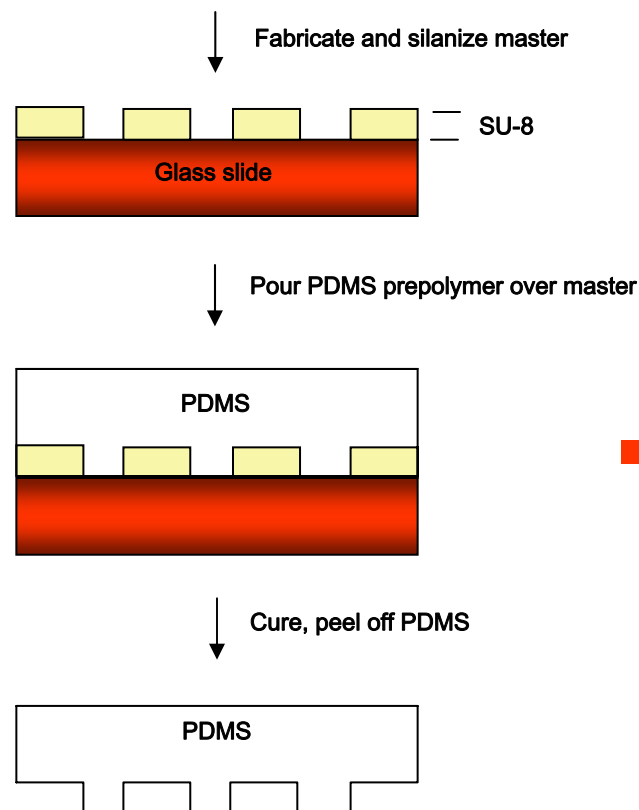


- *E. coli* assay

- Target antigen: *E. coli* (ATCC 15597)
 - Cultured in trypticase soy broth at 37°C for 12 hours
 - The strain of *E. coli* grew to stationary phase
 - Grown *E. coli* culture was diluted with dechlorinated tap water by 10^{-3}
- Counting *E. coli*
 - Planting 0.01 ml of diluted samples to tryptic soy agar plate and incubating at 37°C for 18 hours
 - Counting viable and non-viable cells: 0.2 ml of 0.1% acridine orange was added to diluted *E. coli* sample. Viable *E. coli* was confirmed through green fluorescence.

• Fabrication of microfluidic device

- Microfluidic devices were fabricated using standard soft lithography with PDMS molding technique
- The Y-junction microchannel ($200\ \mu\text{m} \times 100\ \mu\text{m}$)



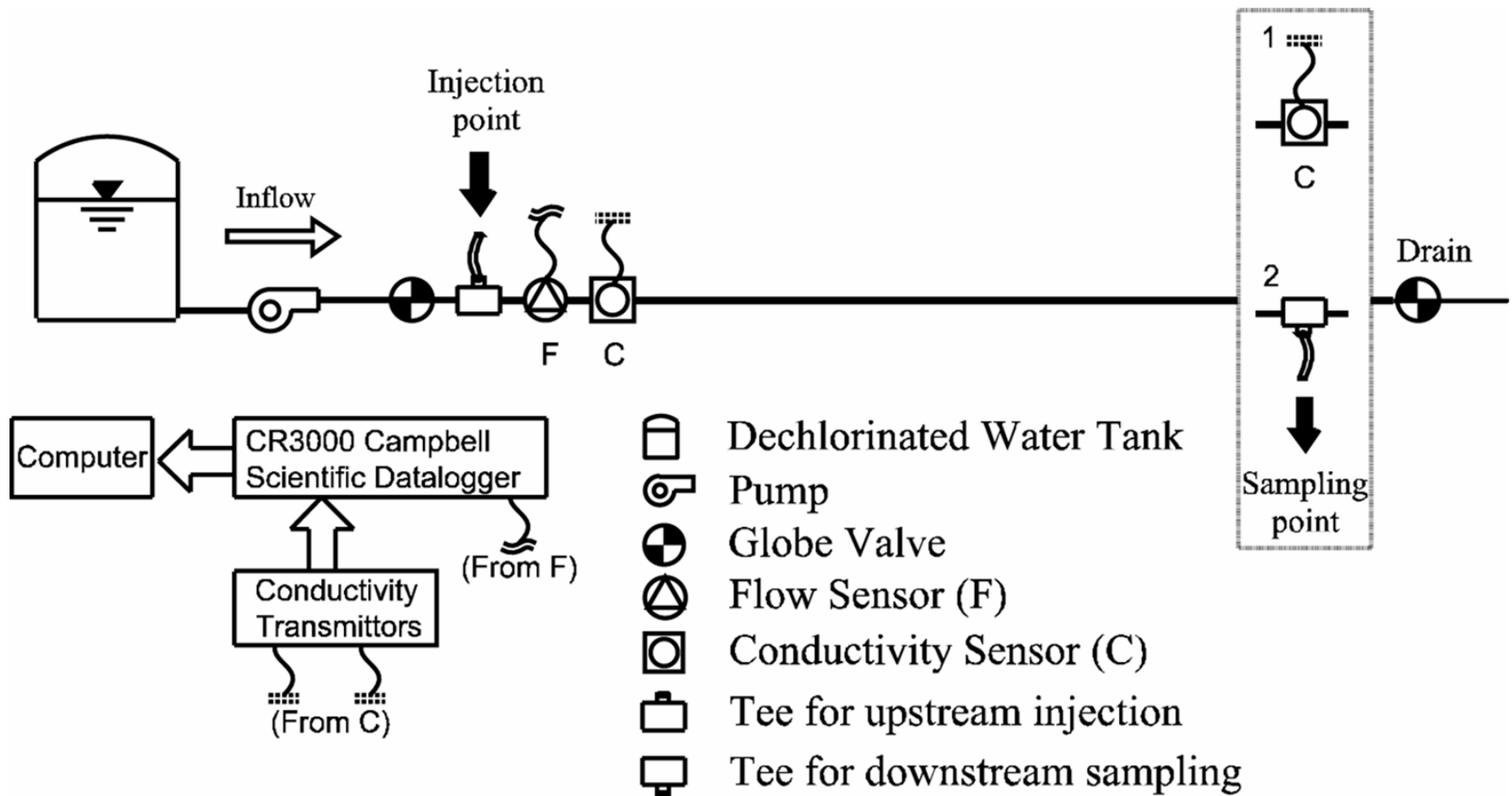
The layout of microfluidic device



• Pipe injection experiment

- A single straight pipe: 8.5 m long, 16 mm inner diameter
- Dechlorinated tap water from a water tank: injected through the pipe system by a centrifugal pump
- Salt tracer: injected through the system at 0.4 l m^{-1} at 10 second pulse using a micro injection pump
- Flow rate: controlled by a valve at the downstream end of a pipe
- Electrical conductivity of salt: measured at both upstream and downstream ends of a pipe using conductivity meters
- The salt tracer concentration: monitored in real time using a data acquisition system
- A series of water samples were collected using a fraction collector at the downstream end of a pipe system, and applied to microfluidic system

• Model pipe system





Optical fibers:
600 μm core
30 μm cladding

Syringe pump

E. coli

Detector

Microparticles
w/ anti-*E. coli*

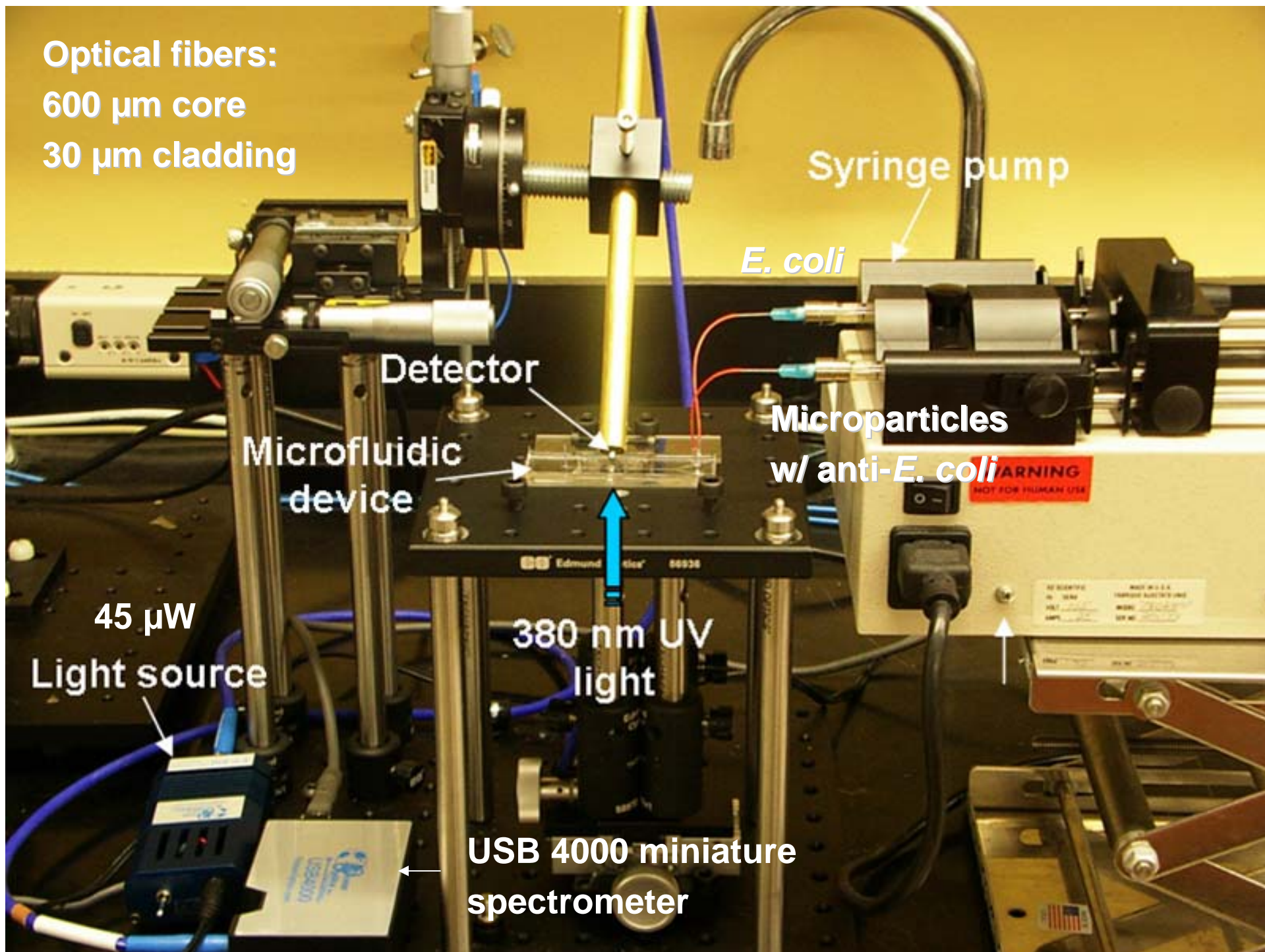
Microfluidic
device

45 μW

Light source

380 nm UV
light

USB 4000 miniature
spectrometer





Results and discussion



• Detection of *E. coli*

	Time (s)	E. coli (cfu ml ⁻¹)	Scattering		Time (s)	E. coli (cfu ml ⁻¹)	Scattering
Laminar	Blank		1217±2	Turbulent	Blank		1253±8
	65	10	1225±4*		17	0	1257±18
	71	10	1232±4*		19	0	1271±5
	77	30	1277±2*		21	48355	1540±15*
	83	12000	1743±37*		23	987331	1669±27*
	89	26000	2350±43*		25	12630566	1939±45*
	95	197000	3044±39*		27	9983316	2102±86*
	101	200000	3541±18*		29	3120125	1607±80*
	107	231000	3930±48*		31	225257	1388±45*
	113	231279	3950±66*		33	58217	1343±35*
	119	64877	3853±66*		36	8509	1313±7*
	140	10697	3376±142*		42	985	1252±33*
	160	10221	3232±22*				
	230	6825	1908±20*				
	300	2985	1282±6*				
RSD (%)	0-4			RSD (%)	0-2		



- Detection range and viability issue

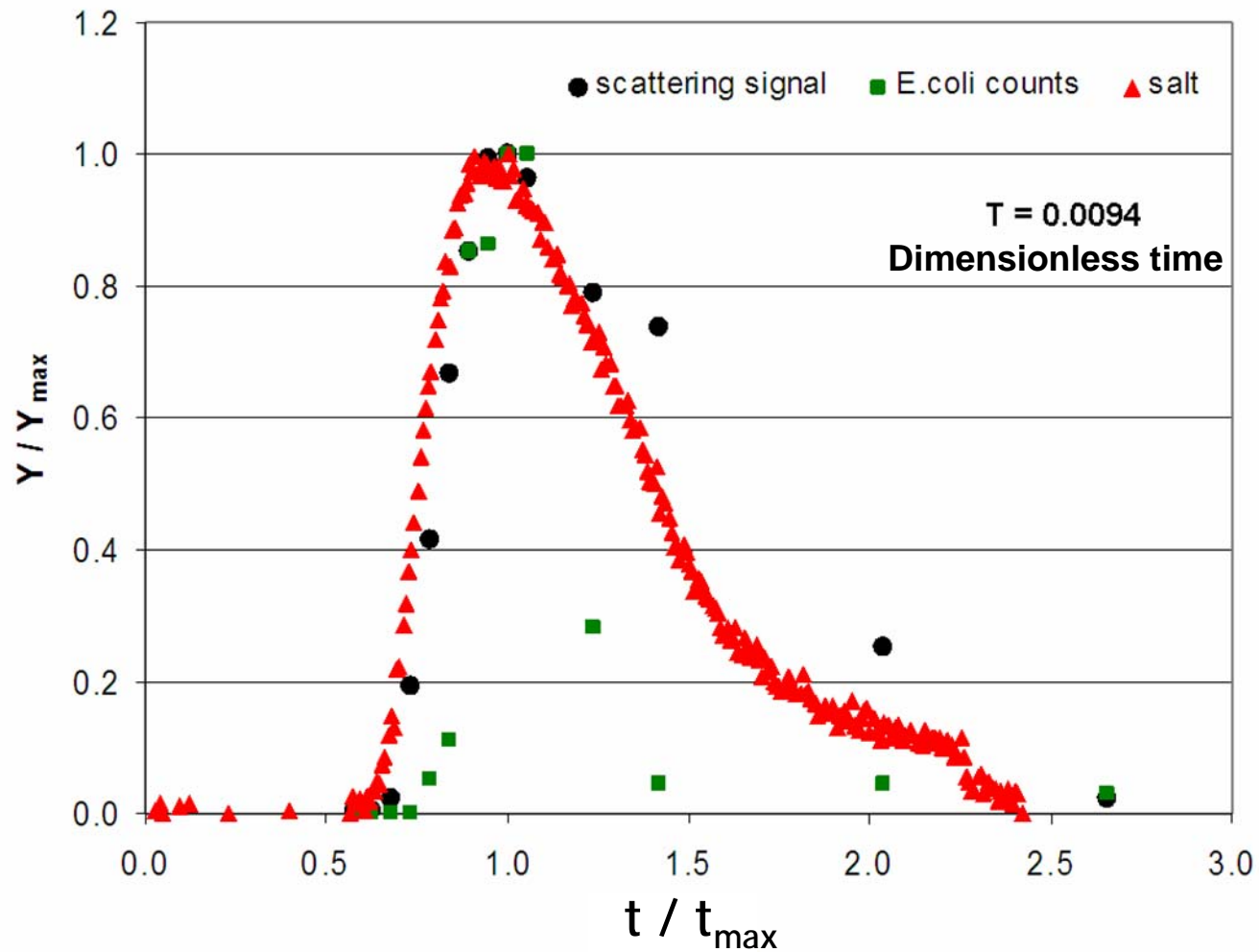
- Detection range

- 10 - 10^6 cfu ml⁻¹ (laminar), 10^2 - 10^7 cfu ml⁻¹ (turbulent)
- Low detection limit: 10 cfu ml⁻¹ (includes not only viable cells but also dead cell and free antigens)

- Detects not just viable *E. coli*, but also dead cells and free antigens

- *E. coli* counts = viable *E. coli* only
- Light scattering signal = viable cells + non-viable cells + free antigens = total *E. coli* (Han et al., *Biosens. Bioelectron.* doi:10.1016/j.bios.2007.11.013, 2008)

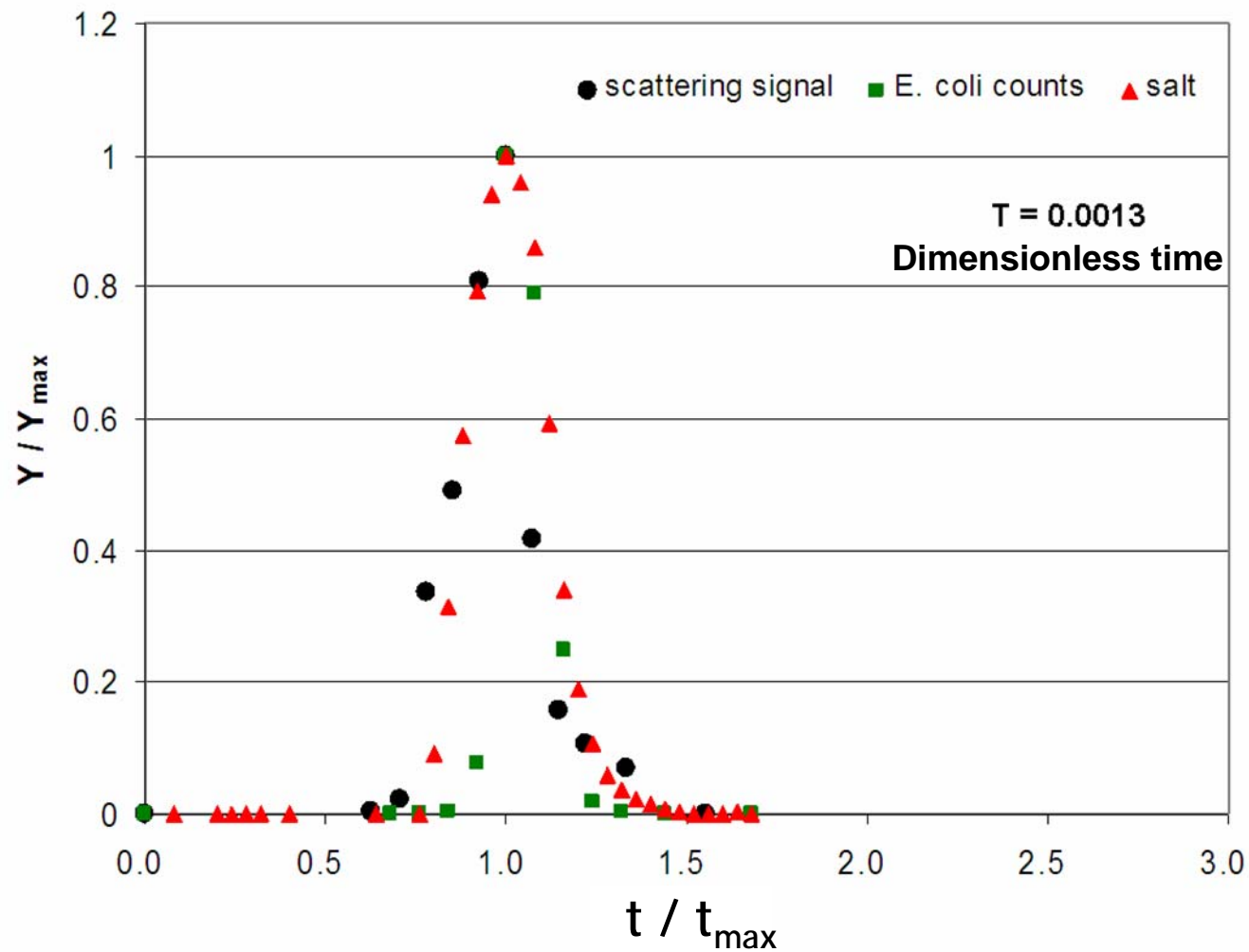
- Axial dispersion of *E. coli* in laminar flow





- Axial dispersion of *E. coli* in laminar flow
 - Total *E. coli* and salt showed almost the same concentration profile (asymmetric)
 - More likely axial convection and axial/radial diffusion, rather than self-motility of *E. coli* or *E. coli* fouling to a pipe wall
 - Viable *E. coli* profile was symmetric
 - Asymmetry originates from non-viable cells and free antigens (i.e. cell fragments)
 - Axial convection and axial/radial diffusion are the issues of cell fragments, not viable cells

- Axial dispersion of *E. coli* in turbulent flow





- Detection range and viability issue
- All three curves showed symmetric profiles
 - Self-motility of *E. coli* do not contribute to the concentration profile
 - *E. coli* fouling to a pipe wall is also negligible



• Conclusion

- *E. coli* could be detected down to 10 cfu ml⁻¹ level in real time
- Cell fragments contributed to axial convection, radial/axial diffusion in laminar flow, just like salts
- Viable cells do not have axial diffusion and radial diffusion issue in laminar flow
- No axial convection, radial/axial diffusion in turbulent flow, for both salt and *E. coli*



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